



Making use of virtual dimensions for visualization and contouring

Haley Clark^{1,2}, Joel Beaudry², Jonn Wu^{1,2}, and Steven Thomas^{2,†} ¹ University of British Columbia, Vancouver, Canada.

² British Columbia Cancer Agency, Vancouver, Canada.

Methods

A prototype viewer was constructed by modifying the free/libre and open source Minetest core [2] and integrated into the DICOMAUTOM-ATON radiotherapy software suite [3]. We refer to it as **DVSM**. Viability of VSM was evaluated with a blinded reproducibility test. Two individuals contoured 10 eyes each using radiotherapy planning CTs, which were compared to professionally-generated planning ROIs. DVSM can be invoked at any point in a standard contouring session (figure 2), so contouring efforts can be split between VSM and CT demarcation onthe-fly; for evaluation purposes entire ROIs were generated using DVSM. A Sørensen-Dice similarity metric (SDS) was used to compare ROIs.

Results

Comparison of DVSM ROIs to planning ROIs resulted in a mean SDS of 0.868±0.005. Comparison between individuals resulted in a mean SDS of 0.889 ± 0.004 . The median-mean SDS percent difference was

> <1% for both comparisons. SDS >0.995 were attained for larger ROIs, (e.g., whole body). It took approximately $4 \times$ longer to contour with DVSM compared with standard CT demarcation.

Discussion & Conclusions

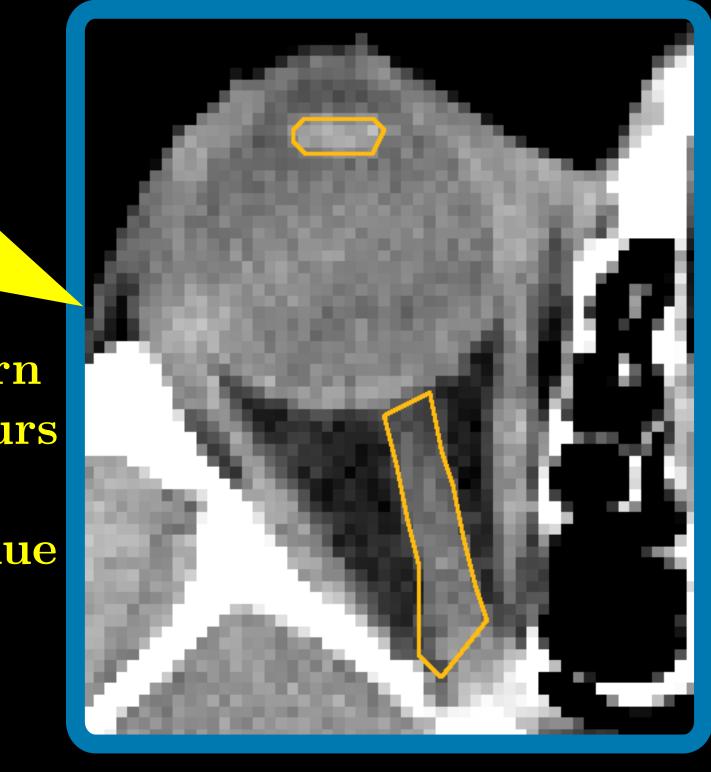
VSM was developed to augment existing methods for displaying images with constrained bit-depths. It exploits innate human geospatial and navigational abilities [4].

DVSM, our prototype viewer, supports windowing, colour mapping, dynamic ranges, and contouring within a virtual 3D environment.

Figure 2: workflow of a DICOM-automaton contouring task (n.b. lens of an eye and part of an optic nerve) being deferred to DVSM. Colour and depth cues are

used. Contouring is accomplished by





Return contours and continue

Contour in a 3D world

Figure 1: a prototype implementation of the proposed 'volumetric slice mapping' technique.

Introduction

Radiotherapy regions of interest (ROIs) are generated by manually demarcating tissue or object boundaries on planar images. Image modalities commonly used (e.g., magnetic resonance imaging, x-ray imaging, computed tomography) produce single-channel images with bit-depths of 16 bits per pixel or greater, which are generally presented in greyscale. Medical displays and computer monitors offer reduced bit-depths of 8-12 bits per pixel, or 256-4096 shades of grey. Kimpe et. al [1] estimate

that human eyes are capable of differentiating only 700-900 shades in ideal conditions. It is therefore not possible to display or differentiate the full range of most medical images. ROI generation is impacted.

Various techniques have been concocted to address this issue. The most common is windowing, in which a subset range is compressed and specific tissues are exaggerated. Another is colour mapping wherein a subset range is replaced

using a colour look-up table. The latter permits a larger range of values to be displayed owing to the high sensitivity of human eyes to colour, but can introduce problems stemming from non-linearity and perceptual differences. Both techniques are commonly used.

Standard contouring task (left eye)

Defer DVSM

Screen

We propose an alternative display technique, Volumetric Slice Mapping (VSM; figures 1, 2), that: incorporates windowing and colour mapping; exploits inherent human geospatial navigational abilities; naturally permits the addition of other visual cues; and is well-suited to interactive tasks such as radiotherapy contouring. Eval-

Similarity coefficients for orbits were consistent across all comparisons. Performance on larger structures increased. DVSM contouring took longer than CT demarcation; however, DVSM is designed to augment CT demarcation, not replace it. Optimizations (e.g., coupling with autosegmentation, additional virtual cues) would ameliorate timing differences and may improve ROI quality [5]. Oblique image slices, time series, and all popular (scalar) imaging modalities are presently supported.

References

1. Kimpe T., and Tuytschaever T., 2007. DOI: 10.1007/s10278-006-1052-3. 2. Ahola P., et. al, Minetest.net. N.p., 2016. Web. 20 Jan. 2016.

3. Clark H., et. al, 2014. DOI: 10.1088/1742-6596/489/1/012009 & references therein. 4. Wang R., and Spelke E., 2002. DOI: 10.1016/S1364-6613(02)01961-7.

uation of the method was performed by testing reproducibility of a

basic contouring task (an eye) using a prototype implementation.

5. Yang J., et. al, 2013. DOI: 10.1016/j.prro.2013.01.002.

The authors acknowledge financial support from the UBC, the BCCA OaSIS project, and the Walter C. Sumner Memorial Foundation.

Poster presented @ ICCR 2016. WWW.HALCLARK.CA/DICOMAUTOMATON Email: hdclark@phas.ubc.ca